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# Pulp dentin complex review pdf online software

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Biomech. the dimensionless time t\* are compared with the values predicted by Equation (6). • Molecules/ions that enter a dentinal tubule do not react with each other. L., Smith, J. doi: 10.1007/s12575-009-9008-x PubMed Abstract | CrossRef Full Text | Google Scholar Gao, Y., Haapasalo, M., Shen, Y., Wu, H., Li, B., Ruse, N. How is the biocompatibility of dental biomaterials evaluated? Fluids 26, 7–15. Figure 5A, which presents the therapeutic agent concentration at the bottom of the dentinal tubule, i.e., at the dentin-pulp junction, as a function of time, demonstrates the effect of initial substance concentration on the concentration change. Online 11, 32–51. A syringe pump (ALLADIN 2000) was employed for the suction of the two liquids inside the capillary (Figure 2). Hargreaves, H. Oral Patol. It is, therefore, desirable to be able to suggest a new integrated computational approach that could adequately simulate both the fluid flow and diffusion characteristics inside the tubules. (1999). V., and Harilal, S. Diffusion coefficients of several rhodamine derivatives as determined by pulsed field gradient-nuclear magnetic resonance and fluorescence correlation spectroscopy. It has been previously documented that large molecules such as endotoxins (1–30 kDa) or exotoxins (20–70 kDa) can dissolve in the dentinal fluid and diffuse to the pulp (Pashley and Matthews, 1993). An example on the application of the proposed methodology is given in the stepwise procedure. (2009). where Rmin is given in nanometers and the molecular weight Mw in Daltons (Da) and where  $k = 1.38 \times 10^{-16} \text{ g cm}^2 \text{ s}^{-2} \text{ K}^{-1}$  is the Boltzman's constant and T the absolute temperature. Smear layer: overview of structure and function. Image processing and concentration calculations were performed using appropriate software (Flow Manager by Dantec Dynamics). Med. Comparison between CFD data and the corresponding results from Equation (3) for: (A)  $t = 0.5 \text{ h}$  and (B)  $t = 3.5 \text{ h}$  after the diffusate release. After the experimental measurements, appropriate numerical simulations that fully represent the initial experimental conditions are performed. The CFD simulations concerning mass transfer of chemical compounds confirm that: • the diffusion is a very slow process, a fact verified by clinical observations, • large molecules penetrate at a lower rate inside the dentinal tubules compared to smaller ones, • the mass flux inside a tubule increases by increasing the initial concentration of the substance and • the time required for the concentration of the signaling molecules to attain a predefined value at the pulp can be controlled by their initial concentration. This is an important finding, especially for the dental community, since it gives the possibility to predict the behavior of each therapeutic agent prior to its application on the dental clinic practice. E. Oral Biol. Effect of the excitation source on the quantum-yield measurements of rhodamine B laser dye studied using thermal-lens technique. Exp. J., Windsor, L. Prof. Thus, an effort was made to propose a simple correlation that could predict with reasonable accuracy the temporal concentration value at the pulp through the dentinal tubules, as a function of the diffusion coefficient of the substance, i.e., its molecular size. However, this is not a trivial procedure to be used in every day practice. 43, 382–392. 132, 482–491. Biomaterials 35, 2890–2904. During the last decades the clinical practice has been oriented toward the design and development of modern dental treatment techniques that would ensure the long-term maintenance of vitality and function of the dentine-pulp complex (de Peralta and Nör, 2014). The experimental study of the diffusion rate of therapeutic molecules inside the dentinal tubules is almost impossible using the established experimental techniques due to the minute dimensions of the dentinal tubules. For each concentration Ci an image C(x, y) is taken. 29, 341–346. As the study comprises the time-dependent solution of diffusion, all simulations were run in transient mode. O., Avaltroni, F., and Wilkinson, K. For example, BMP-7 is such a bioactive protein used in the dental clinic practice with approximately 50 kDa molecular weight and Rs of 2.2 nm. Stepwise procedure Ci in the present protocol study is a stepwise procedure for estimating the diffusate concentration to be imposed at the dentin-enamel junction so as the drug concentration to attain a required value at the pulpal side of the tubules is proposed given the geometrical characteristics of the dentinal tubules. • Estimate the diffusion coefficient of the agent through Equations (4, 5), given its size or molecular weight. Laser-Induced Fluorescence (LIF) is an optical measuring technique used to measure instant whole-field concentration maps in liquid and gaseous flows. Whole field measurement of temperature in water using two-color laser induced fluorescence. Oral Cir. In steady state conditions the diffusive flux j of a substance driven by the concentration gradient in one dimension is given by the Fick's First Law (Equation 1): where j is the flux, D is a diffusion coefficient,  $\partial C/\partial x$  is the concentration gradient and x is the distance in the direction of transfer. "Regeneration of the living pulp," in The Dental Pulp, ed M. H. As already mentioned, for the experimental study of the diffusion in  $\mu$ -channels and for validating the CFD code, the non-intrusive micro Laser Induced Fluorescence ( $\mu$ -LIF) technique was employed. The local dye concentration is measured by the non-intrusive  $\mu$ -LIF measuring technique and the acquired experimental data are compared with the CFD results. The initial mass of the diffusate is located at  $x/L = 0$ . Endof. For studying the transcendental diffusion, we use substances whose molecular sizes are the same as those of potential therapeutic agents that are used in dental clinic practice. Figure 3. The numbers of odontoblasts surviving the injury caused by the cavity cutting and restoring procedures have been strongly correlated with cavity preparation technique and dimensions, the nature of tested materials including the diffusion rate of their components, and method of application (Smith et al., 2001). We must point out here that our study deals with a sole microtube that represents a typical dentin tubule that bears no obstructions of any type. Comparison of CFD data with the corresponding results from the LIF technique: (A) mass concentration distribution inside the capillary after  $t = 4 \text{ h}$  and (B) mass concentration values for  $x/L = 0.067$  and 0.330; error bars:  $\pm 10\%$ . Development of several in vitro approaches simulating clinical conditions that are helpful to control parameters concerning experimental conditions is in progress during the last two decades. Diffusion is the net movement of a substance from a region of high concentration to a region of low concentration, i.e., it is the movement of a substance down a concentration gradient. Figure 2. (2007). In this case one must run the relevant CFD simulation to produce an appropriate curve like the one presented in Figure 5. Dent. • As the required effective drug concentration (Cr) is dictated by the dental clinic practice, the final concentration (Cf) can be calculated as  $Cf = Cr/0.25$ . The measuring section was illuminated by a double cavity Nd:YAG Laser emitting at 532 nm. Among other issues, the simulation of clinical conditions requires the development of an experimental methodology that can calculate the transport rate of selected molecules by employing advanced non-intrusive techniques. doi: 10.1016/j.joen.2009.06.018 PubMed Abstract | CrossRef Full Text | Google Scholar Gendron, P. After the calibration of the measuring system, the two liquids, namely water and the colored aqueous solution at  $C = 0.05 \text{ mg/L}$ , were successively inserted into the capillary. Murray et al. The radius Rs of their molecules is in the range of 2.2–2.20 nm and consequently the corresponding diffusion coefficient, D, in water at 37 °C is in the range of 1.36–0.14–10–10 m<sup>2</sup>/s. The proposed correlation, given in Equation (6), has been formulated by data fitting on the computational results and incorporates the dimensionless time t\*:  $C/Ci = \exp(0.21 + 0.115t^* \ln(t^*))$  (6) In Figure 6 the computational results concerning the dimensionless concentration at the pulpal area vs. Previous data have showed that diffusion rate of dental material components exerting possible toxicity to the pulpal cells depends on the remaining dentin thickness. Graphical solution of Equation (6), M. Model. Table 1. The LIF experimental setup, available in our Lab, is shown in Figure 1. In a previous experimental approach we reported that TGF- $\beta$ 1, and to a lesser extent, BMP-7 provided evidence that stimulate tertiary dentin, while intratubular mineralization may occur when these growth factors are placed on deep dentine cavities (Kalyva et al., 2010). Therefore, Computational Fluid Dynamics (CFD) seems to be the only feasible method for studying the problem under consideration. Endodont. (1992b). This research has been co-financed by the EU (ESF) and Hellenic National Funds Program "Education and Lifelong Learning" (NSRF)-Research Funding Program: "ARISTEIA"/"EXCELLENCE" (grant no 1904). References Bindhu, C. (2010). It is worth noting that the time required for the concentration of signaling molecules to attain a specific value at the pulp can be controlled by their initial concentration. doi: 10.1016/0003-9969(93)90122-3 PubMed Abstract | CrossRef Full Text | Google Scholar Sakakibara, J., and Adrian, R. • If it is desirable for the required drug concentration value to reach the pulp within 2 h, the variable t\* = 0.15. Figure 4. Sci. Restorative pulp and repair responses. A time-step dependent study was also
performed, to ensure that a suitable time step is selected for each simulation, i.e., the minimum number of calculation steps performed without jeopardizing the accuracy of the solution. However, the overall dentin permeability may be reduced due to occlusions of one or more dentin tubules and for this reason one must be able to apply a typical value (i.e., coefficient) of potential permeability, but this is beyond the scope of the present study. Rs, called Stokes radius, represents the radius of a smooth sphere that would have the same frictional coefficient  $\zeta$  with a protein and is expressed in centimeters in this equation. Murray, P. In the present study we propose a simple algorithm which, given the type of molecules of the therapeutic agent and the maximum acceptable time for the drug concentration to attain a required value at the pulpal side of the tubules, can estimate the initial concentration to be imposed. Development and validation of a three-dimensional computational fluid dynamics model of root canal irrigation. PubMed Abstract | Google Scholar Smith, A. Since it is reasonable to suggest that any toxic interruption or therapeutic up-regulation of the biosynthetic activity of odontoblasts (Smith, 2003) will probably reflect the molecular concentration of these constituents at the dentin-pulp interface area, a number of delivery considerations might be firstly addressed. Anticipated Results The diffusion of a substance similar to the therapeutic agent BMP-7, through a dentinal tubule under different values of initial concentration has been studied. 36, 33–43. To conduct a parametric study, three initial concentration values for each diffusing substance are also employed, namely 0.10, 0.05, and 0.01 mg/mL. The main assumptions made are: • The geometry comprises a typical dentinal tubule 2.5 mm long and 1 and 3  $\mu$ m in diameter at the dentin-enamel and the dentin-pulp junction respectively. They concluded that an RDT greater or equal to 0.5 mm is necessary to protect the underlying odontoblasts from the operative trauma. This paper tackles the problem of substances through a conical  $\mu$ -tube that simulates a typical dentinal tubule. doi: 10.1047/10143-2885.2003.00609.x PubMed Abstract | CrossRef Full Text | Google Scholar Pashley, D. The experiments were performed in a glass capillary (ID = 580  $\mu$ m,  $\mu = 3 \text{ cm}$ ). The discrepancy between the two methods may be attributed to the fact that the experimental data concerning the mean concentration values that were measured at the applied ROI, while the corresponding values from the CFD results give the concentration at the center of a grid cell with an axial dimension of 5  $\mu$ m. 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The present work is part of an ongoing investigation on phenomena related to the dental therapeutic approach and is expected to be published in the near future. doi: 10.1016/j.joen.2009.06.018 PubMed Abstract | CrossRef Full Text | Google Scholar Pashley, D. The experiments were performed in a glass capillary (ID = 580  $\mu$ m,  $\mu = 3 \text{ cm}$ ). The discrepancy between the two methods may be attributed to the fact that the experimental data concerning the mean concentration values that were measured at the applied ROI, while the corresponding values from the CFD results give the concentration at the center of a grid cell with an axial dimension of 5  $\mu$ m. It is therefore quite reasonable to assume that the validated computational code can be applied for studying the diffusion of substances similar to potential therapeutic agents through a typical dentinal tubule. 1, 19–49. E., Garcia-Godoy, C., and Garcia-Godoy, F. 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